



Inhaler Technology

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Introduction

Inhalers are a commonly used device to deliver medication to individuals with airway disease. With correct use, inhalers are very effective at providing quick and effective symptomatic relief within the lung, avoiding high levels of systemic exposure. These pharmacokinetic characteristics widen the therapeutic index, thus allowing for maximal therapeutic benefit with minimal adverse effects. However, this theoretical advantage is somewhat attenuated by incorrect use of the inhaler device. Improper usage of inhalers facilitates oropharyngeal deposition which significantly increases systemic absorption of the drug resulting in increased toxicity. For example, when particles that are too large are inhaled, the upper throat deposition of corticosteroids causes hoarseness and oropharyngeal candidiasis; by contrast, increased alveolar deposition of much smaller particles can cause an increase in systemic adverse drug reactions.

Inhalers, therefore, play a crucial role in the management of patients with airway disease and it is being recognised that the choice of the inhalation device appears to be as important as that of the drug molecule. Indeed in daily clinical practice, pulmonologists usually focus on the pharmacological properties of the various respiratory drugs in selecting the best possible therapeutic option, but little consideration is given to the features of the different inhalers and to the ability of the patient to use the device itself. In fact, it is often underappreciated how incorrect inhaler usage by patients is directly associated with increased healthcare resource utilisation [1].

Furthermore, with increasingly constrained societal healthcare budgets and expiring patent protection for many branded medications, there is emphasis on the development of generic inhaled drugs that are therapeutically equivalent to the original registered products, but may differ in their formulation and the design of the inhalation device. This growing scenario poses practical clinical questions about the potential impact of switching from branded to generic inhaler products in managing patients with airway disease. Indeed, the estimated 10 new drug product launches in COPD over the next 2 years will lead to even more confusion in respiratory prescribing, as there are currently more than 250 inhaler products in pharmaceutical formularies and direction is greatly needed to help healthcare professionals advise and prescribe the 'appropriate' inhaled drug/device product for their patients [1].

This article aims to provide the importance of the inhaler device in the management and treatment of patients with airway disease, and specifically to provide information to support decisions on the appropriate choice of device by healthcare professionals [2-4]. It also addresses and contrasts the advantages and limitations of different available inhalation device options.

Principles of Operation

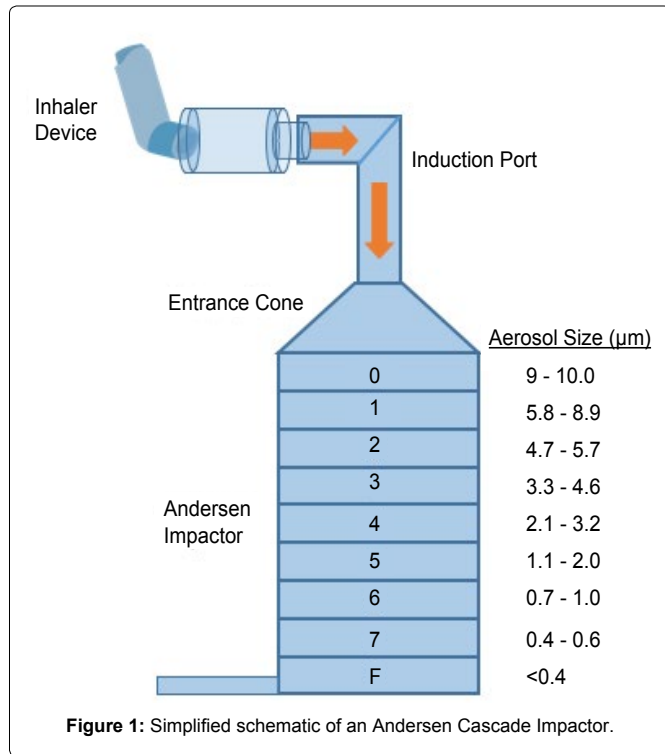
A pneumatic nebuliser requires a pressurised gas supply as the driving force for liquid atomisation; the compressed gas is delivered through a high velocity jet which creates an area of negative pressure at the periphery of the jet stream (also called the Venturi effect). The solution in the reservoir is introduced into the gas stream and is sheared into an unstable liquid film which breaks into droplets due to the surface tension forces. Therefore, a baffle is placed in the aerosol stream which produces smaller particles causing larger particles to return to the reservoir. The aerosol produced is then delivered to the patient.

The degree of size variability between particles in an aerosol is vital for evaluating inhaler devices. This is either assessed using the mass median aerodynamic diameter (MMAD), which is the particle size (mass) below which 50% of the particle population lies, or the fine particle fraction (FPF), which is the fraction of the total drug dose < 5.8 µm in aerodynamic diameter [5]. The key characteristic of an aerosol is the particle size, with the ideal diameter falling between 1 and 5 µm with a narrow monomodal distribution. While the MMAD locates the central point of the particle size distribution, the geometric standard deviation (GSD) describes the spread of the particle size distribution, both of which are important in assessing the particle output from an inhaler device [6].

The Andersen Cascade Impactor (ACI) is the standard technique used to assess aerosolized particle size and distribution emitted from an inhaler device [7]. The ACI is an 8-stage cascade impactor with the stages typically assembled in order of decreasing particle size [8]. This allows the device to collect samples in a graduated manner. Each stage consists of a series of jets that direct any aerosolized particles towards the surface of a collection plate. If a particle has adequate inertia, which is directly related to its aerodynamic size, it will impact on the collection plate, otherwise it will remain trapped in the airstream and pass to the next stage to repeat this process [8]. The smallest particles are trapped by a final filter. This is a relatively primitive technique

that cannot account for the effect of varying time constants within the lung of patients with significant airway disease. These uneven time constants will result in variable distribution throughout the lungs and the issue of deposition is further complicated by the presence of secretions and mucus that will block the passage of aerosols through the lung. An ACI is illustrated in figure 1.

The tagging of radioisotopes to the particles does allow for better in-vivo estimation via scintigraphy, but this is typically only completed in healthy volunteers and this technique is not applicable



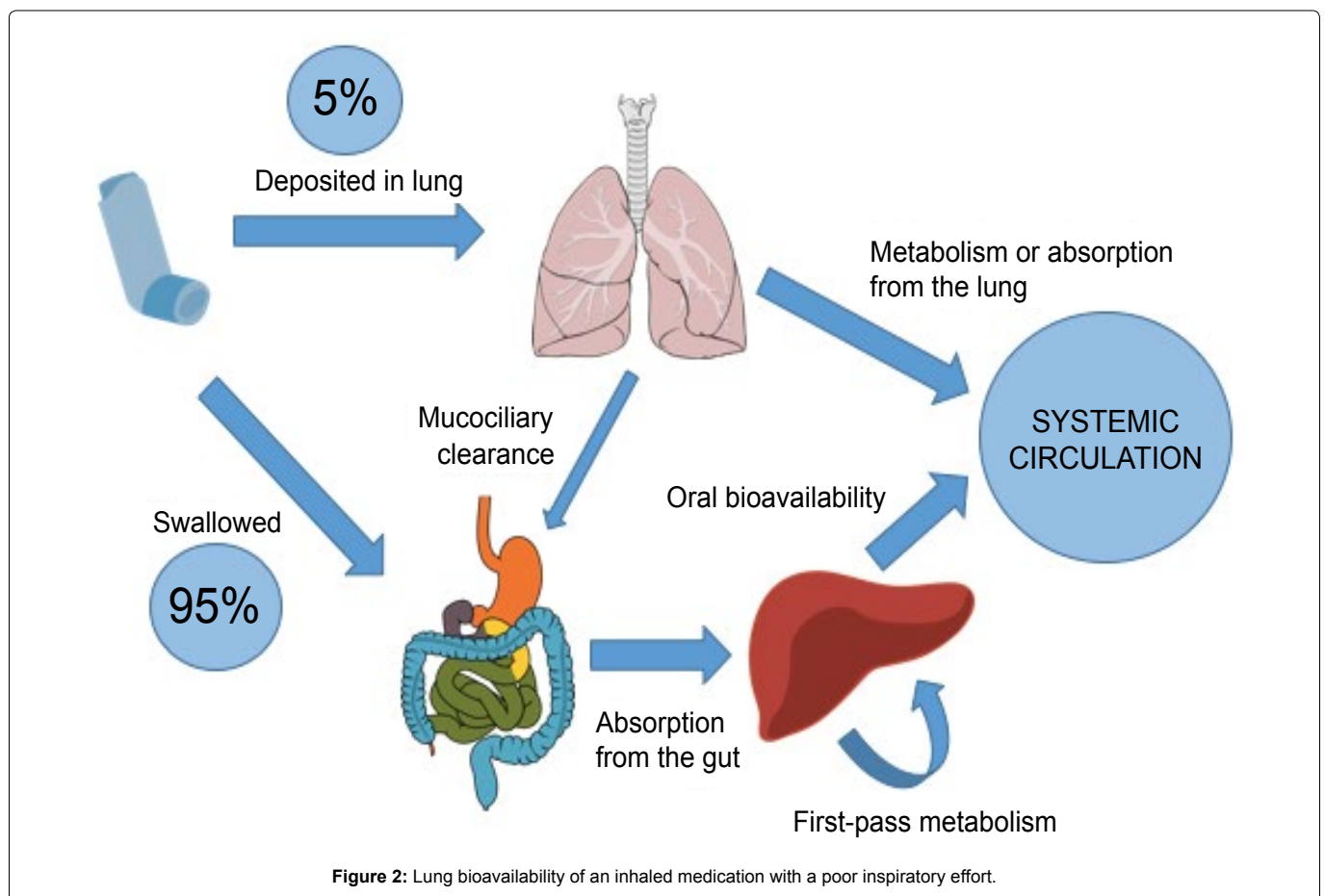
to drugs adherent to lactose carriers (i.e., most dry powder inhalers) [9]. Adequate assessment of dry powder inhaler efficacy is difficult to undertake since the lactose carrier prevents radioisotope attachment in scintigraphy testing. The lung bioavailability of inhaled medications is estimated by asking healthy volunteers to ingest activated charcoal which blocks oropharyngeal absorption therefore eliminating systemic drug absorption via this route. What these studies have shown is that lung bioavailability is significantly decreased with improper technique of inhalers, which can reduce lung deposition to as little as 5 percent from an average of 20 percent [10-16]. This is highlighted in figure 2.

Types of Inhaler Devices

Inhaler technology is currently used to administer an extensive list of medications, including glucocorticoids, beta-agonists, anticholinergics, certain antibiotics and even insulin, directly to the lungs. And even though new inhaler technology is continuously being developed, currently available inhaler devices can be largely classified as belonging to one of three main categories: the dry powder inhaler (DPI), the metered dose inhaler (MDI), and the nebulizer.

Dry powder inhalers

DPIs were developed to provide an alternate solution to MDIs in the management of airway disease. DPIs are composed of a dry powder suspension that becomes fluid on inhalation [17]. These specialized inhalers require drug micronization and combination with a carrier particle to achieve adequate therapeutic benefit [18]. The process of micronization produces a particle with a MMAD of less than 5 μm that readily deposits in the lungs [19]. Due to the large cohesive forces that exist between such fine particles, disaggregation is difficult and requires a large carrier particle such as lactose to assist in particle separation [17,18]. As the patient inspires, turbulent forces convert the dry powder formulation to a fluid that enters the airway [17]. Finally, to achieve deposition in the lungs, a large inspiratory flow rate is required to separate the drug particles from the lactose carrier [9,17,18].



The inspiratory-dependent technology of DPIs eliminates synchronization between inspiration and inhaler administration that is required with traditional MDIs [20]. This is advantageous as it assists in minimizing the oropharyngeal deposition that occurs with improper coordination of MDIs [21]. Additionally, DPIs are a most sustainable device as they do not contain propellants and operate at lower states of energy which decreases reactions occurring between the inhaler chemicals and extrinsic surfaces [17]. Although DPIs have the potential to be advantageous in certain scenarios, the requirement of a large inspiratory flow rate (between 30 to 60 L/min) to assist in drug activation limits the use of DPIs to patients with adequate pulmonary function [18-20,22].

Future studies are currently examining the possibility of reducing the dependence of DPIs on inspiratory flow rate which can potentially allow DPIs to be very effective devices in the management of airway disease [17,18,23]. However, it should be noted that the idea of a low resistance device may be misguided because a certain amount of resistance is inherently required to ensure disaggregation of the drug from the lactose carrier; therefore, oropharyngeal deposition may occur because of the inadequate disaggregation [23,24].

Metered dose inhalers

MDIs can be further classified as either a pressurized (contains propellant) or a non-pressurized (does not contain propellant) device.

Pressurized metered dose inhalers: Developed in 1956, the pressurized metered dose inhaler (pMDI) was the first type of inhaler device to be marketed for the treatment of airway disease. It is both the most cost-effective type of inhaler device and the most widely used [25]. Basically, a pMDI device consists of a metering valve and stem, a mouthpiece actuator, and a pressurized canister containing a medication suspended within a propellant [26]. The propellant is a liquefied compressed gas that can maintain a constant vapour pressure, which is essential for proper device functionality as it allows for a consistent suspension pressure regardless of the volume remaining in the canister. Otherwise, the pressure would change with each use of the inhaler, thus severely limiting the effectiveness of the device [26].

Initially, pMDI devices contained chlorofluorocarbons (CFCs) as a propellant, but they have since been replaced by the CFC-free propellant hydrofluoroalkane (HFA). This was following the implementation of the 1987 Montreal Protocol – an international agreement to ban CFCs due to their documented role in ozone depletion [25,27-30]. This change in propellant, however, has not negatively impacted the capability of pMDI devices to adequately deliver inhaled medications to the lungs [30-33]. Furthermore, studies have shown that some HFA devices may deliver a higher fraction of the inhaled dose when compared to similar CFC devices [27,34-36].

This finding may be explained by the tendency of HFA-containing pMDIs to produce much softer and warmer plumes, resulting in less oropharyngeal deposition [37,38]. Moreover, the warmer plume decreases the number of patients experiencing a phenomenon known as the ‘cold freon’ effect, which is a cold sensation felt at the back of the throat following device actuation. This is most likely a result of the forceful plume impacting on the back of a patient’s throat [37]. Interestingly, when HFA-containing devices were first introduced, many patients felt that the new inhalers were not actually working properly due to the absence of this so-called ‘cold-freon’ effect. Patients had associated this phenomenon with the effectiveness of the inhaler, therefore proper education was required to address this misconception [37].

Another benefit of many HFA-containing pMDIs is that the active drugs are in a true solution as opposed to a micronized suspension. Therefore, the drug particles will not settle in the propellant, eliminating the need to shake the device before each use [39]. With CFC devices, shaking the device was of utmost importance as improper dispersion of the suspension could reduce the delivery of some medications by up to 50% [39-42].

Breath-actuated pMDIs: Breath-actuated pMDI (BA-pMDI) devices are a newer generation of inhaler technology designed specifically to address the issue of poor actuation-inhalation coordination and thus improve patient compliance and confidence [43,44]. Similar to a conventional pMDI, these devices contain a pressurized canister, however, a spring triggers the canister to release the dose during inhalation and automatically coordinate device actuation with patient inhalation [10]. The patient is required to inhale through the mouthpiece at a low flow rate of 22-36 L/min, which is easily achieved by most patients [10,45].

Non-pressurized metered dose inhalers: The soft mist inhaler (SMI) is a propellant-free type of MDI device that releases a soft-mist of medication. Roughly 75 percent of the aerosolized particles produced by SMIs have a MMAD \leq 5.8 μ m, while approximately 5 percent of the particles have a diameter $<$ 1 μ m [46]. This soft-mist has a lower velocity and thus remains in the air for approximately seven to ten times longer than the aerosol from a typical pMDI, significantly reducing the amount of synchronization required to successfully operate the device [47]. This results in decreased oropharyngeal deposition while also increasing the window for successful inhalation [46,48]. Furthermore, a lower nominal dose is required to achieve the same therapeutic effect as a typical pMDI [47]. Scintigraphy studies have shown that SMIs achieve greater lung and lesser oropharyngeal deposition when compared to both DPIs and pMDIs [49,50].

Nebulizers

Nebulizers are a type of inhaler device that aerosolizes a solution of medication using compressed gas, a mesh, or ultrasonic waves. Depending on patient preference, the aerosol can then be administered by a facemask, mouthpiece or potentially a nasal cannula. Presently, there are three main types of nebulizer devices: jet, mesh, and ultrasonic.

Jet nebulizer: Jet nebulizers produce an aerosol by delivering a jet flow of compressed air or oxygen through a narrow opening, creating an area of negative pressure directly above a reservoir of medication [51]. This is known as the Venturi effect – the reduction in fluid pressure that results when a fluid flows through a constriction. The resulting suction that is created pulls the solution into the gas stream, generating an aerosol [52]. The droplets generated by this primary process have a mean size that ranges widely between 14 μ m and $>$ 500 μ m [53]. A baffle placed in the aerosol stream helps ensure the formation of respirable particles (1 to 10 μ m), while simultaneously preventing the inhalation of larger droplets [53].

Mesh nebulizer: Mesh nebulizers are portable, battery operated devices that produce a liquid aerosol by forcing a solution of medication through a mesh or plate with multiple apertures [54]. This avoids the requirement of a compressed air source or an internal baffling system. The particle size and FPF are all functions of the exit diameter of the aperture hole (approximately 3 μ m in some devices), which can be adjusted to suit different clinical applications [55]. Furthermore, these devices typically generate aerosols with a high FPF compared to conventional jet or ultrasonic nebulizers, thus improving their ability to deliver drugs to the lower respiratory tract [55].

Ultrasonic nebulizer: Ultrasonic nebulizers convert electrical energy into high-frequency ultrasonic waves using a power unit. The high-frequency ultrasonic waves then stimulate the mechanical vibration of a piezoelectric element in the transducer. This transmits the high-frequency vibrations to the surface of the liquid reservoir to create an aerosol [56]. The aerosol is then delivered to the patient using an electric fan or the patient’s own inspiratory effort. The droplets produced by ultrasonic nebulizers tend to contain particles with a higher MMAD (approximately 1 to 6 μ m depending on the manufacturer) than particles from a jet nebulizer [52]. Particle size is inversely proportional to the frequency of the ultrasonic waves. However, it should be noted that ultrasonic nebulizers produce a heating effect (1 to 2°C) which may denature thermally sensitive drugs such as proteins and therefore are not suitable for nebulising

some suspensions, for example DNAses [57]. Experimentally it has been shown that cooling in combination with a surfactant is one potential approach to stabilizing proteins for ultrasonic nebulization, but this also significantly reduces device output [57].

Spacers and Holding Chambers

Spacers and valved holding chambers were designed to reduce the amount of drug lost to peripheral deposition when using MDIs [19]. Both spacers and valved holding chambers function to decrease the velocity and size of drug particles prior to arrival at the mouth, which results in increased drug bioavailability and a reduction in particle loss due to external deposition [23]. Additionally, the unique design of valved holding chambers eliminates the requirement for proper coordination between patient inhalation and actuation of an MDI device [17,20]. This is advantageous as improper inhaler technique is a large contributing factor in oropharyngeal deposition. Caution must be taken with the use of spacers as exhalation into the device prior to drug inhalation can dilute the medication dose. This dilution effect is not seen with valved holding chambers due to the presence of a valve between the chamber and mouthpiece that prevents the entrance of exhaled breath into the chamber [17].

While these tools provide effective solutions to issues that arise with MDI usage, these advantages come at an additional burden to the healthcare system [20]. Their large and bulky nature also eliminates the portability of the inhaler device which is one of the main advantages of MDIs [20,23]. Additionally, the large size of a spacer or holding chamber may, to some extent, prevent the immediate use of an inhaler in a time of crisis [20].

Technology Limitations

The key issues associated with the use of inhaler devices are insufficient coordination between actuation and inhalation, oropharyngeal deposition, and to a lesser extent, poor breath-hold after inhalation.

Actuation-inhalation coordination

Inadequate coordination between actuation and inhalation is a significant cause of poor delivery of inhaled medications to the lower airways, especially in children and the elderly. This problem can be avoided through the use of a valved holding chamber as described previously or a breath-actuated DPI device. More recently, BA-pMDI devices have been designed that solve the issue of patient coordination [58]. These breath-actuated devices actually sense the patient's breath through the actuator and automatically synchronize device actuation with inhalation. Studies have shown that patients generally prefer the BA-pMDIs over the conventional devices as they find them simpler to operate [59,60].

Upper airway deposition

MDI devices generally deliver an aerosol plume faster than a patient can inhale, which is further compounded when a patient does not inhale long enough after device actuation [21]. In the case of some DPI devices, patients seldom achieve the maximum force required during inhalation to disperse the powder [38]. These issues result in a significant amount of medication being deposited in the back of the throat or the tongue, i.e., the upper airways. Oropharyngeal deposition can lead to inadequate delivery of medication to the lungs, while also increasing systemic absorption and the likelihood of unnecessary side effects such as oral thrush with inhaled glucocorticoids. Studies have shown that approximately 10 percent of the inhaled dose reaches the lungs of most patients, while 80 percent is deposited in the upper airways [10,26,34,36,38,61].

With respect to nebulizers, the breathing pattern of the patient can significantly affect the amount of aerosol deposited in the upper airways. Patients should be directed to adopt a slow breathing pattern with a normal tidal volume and an occasional deep breath to increase lower airway deposition in the lungs.

Insufficient breath-hold

It is generally accepted that a 5 to 10 second breath-hold is needed at the end of inhalation from either an MDI or a DPI to avoid substantial exhalation of the medication. This is supported by a study assessing lung deposition of HFA - and CFC-beclomethasone using varying breath-hold times that found a 16 percent reduction in lung deposition for a 1 second breath-hold when compared to a 10 second breath-hold [35].

Patient Education

Education and training in inhaler usage for both patients and healthcare professional alike, is an integral part in the management of airway disease. Issues with inhaler technique are extremely common and can lead to poor symptom control as a result. Prescribing inhalers should be done only after patients have received adequate training and have demonstrated proper usage of the inhaler. The British Thoracic Society recommends developing a personalized action plan for individuals suffering from airway disease and ensuring there are adequate trained personnel in practice to facilitate educational demonstrations [62]. Written instructions have proven to be ineffective, but rather, face-to-face or video demonstration (with the physician or with a trained nurse) is more beneficial at ensuring adequate inhaler technique and treatment adherence [63,64]. Placebo inhalers (available from inhaler manufacturers) can help with demonstrating correct inhaler technique, but these placebo devices are for single-person use only. In addition to proper demonstration, periodical follow-up and evaluation of inhaler technique has shown to be essential in ensuring correct usage [19]. Furthermore, printable handouts/flyers that provide information on inhaler technique as well as step-by-step instructions on correct usage of a respective inhaler are readily available.

Future Considerations

While never quite reaching mainstream use due to multiple technical difficulties, the experience with inhaled insulin has shown that the potential to deliver drugs systemically through the inhaled route is a real possibility. Furthermore, the incorporation of light porous particles into dry powder formulations will increase the number of antibiotics that can be delivered through an inhaler device. In the very near future, it is possible that we will be routinely treating bacterial lung infections using inhaler technology. This further emphasizes the importance of proper education to ensure maximal therapeutic benefit.

Conclusion

The advent of inhaler devices revolutionized the management of airway disease. These compact and portable devices facilitate quick therapeutic relief during exacerbations of airway disease while minimizing systemic exposure and the therapeutic dose. A lower dose of drug is often advantageous for medications with a narrow therapeutic index or for drugs which have high toxicity; delivering the medications to the site of action for a localized effect, resulting in a rapid clinical response with few side effects.

While inhalers have proven to be very effective devices, the broad range of devices has the potential to overwhelm physicians when deciphering which one is most suitable for a particular patient. While MDIs have proven to be effective at minimizing oropharyngeal deposition, inadequate coordination between actuation and inhalation decreases the efficacy of this device. Conversely, DPIs have eliminated the need for synchronization between actuation and inhalation, but drug activation requires a large inspiratory flow rate which is not always realistic in patients suffering from airway disease.

With such a diverse range of available inhaler devices, it is imperative that physicians understand not only the pharmacokinetic principles of each inhaler device, but the salient advantages and disadvantages of each device as well. Combining knowledge of inhalers with patient ability will help ensure that the patient is receiving the best therapy possible. For instance, simply being aware

that a patient is unable to produce an inspiratory flow rate between 30 to 60 L/min would discourage a physician from prescribing a DPI that would eventually be proven ineffective. Additionally, having a working knowledge of other devices such as nebulizers, spacers and valved holding chambers is advantageous as these devices can be utilized to minimize the issues associated with traditional MDIs or act as an alternative option to either MDIs or DPIs. Shifting the focus of prescribing based on pharmacological principles to also include prescribing based on physiological principles of inhalers will help ensure better management and potentially minimize exacerbations of airway disease.

Inhalers have proven to be an invaluable tool in the management of airway disease. As the continued burden of inhalers on the healthcare system increases, it is imperative for both the physician and patient to continually educate themselves on the properties of inhalers and proper inhaler technique. Proper inhaler education will help to ensure that a patient is prescribed the most appropriate device to address their healthcare needs.

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