



## Pre-Clinical Pharmacokinetics of Sufentanil-2-Hydroxypropyl-B-Cyclodextrin Inclusion Complex

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### Abstract

This study evaluated the pre-clinical pharmacokinetics induced by sufentanil-2-hydroxypropyl- $\beta$ -cyclodextrin inclusion complex (SUF<sub>HP- $\beta$ -CD</sub>) in comparison with its aqueous formulation (SUF) after intramuscular injection in rabbits and pigs. New Zealand White rabbits and Landrace pigs were divided in two groups (n = 5/6) and treated by intramuscular route with SUF or SUF<sub>HP- $\beta$ -CD</sub> complex (10  $\mu$ g.kg<sup>-1</sup>). Blood samples were collected by a heparinized cannula pre dose (0 min) and at 15, 30, 45, 60, 90, 120, 180, 240, 300, 360, 420 and 480 minutes after the injection of formulations in rabbits and pigs. Sufentanil plasma levels were determined using liquid chromatography-tandem mass spectrometry. Data were submitted to statistical (two-tailed unpaired t-test, p < 0.05) analysis. In both species, intramuscular injections of SUF<sub>HP- $\beta$ -CD</sub> induced lower plasma concentrations than SUF at almost all periods of time (p < 0.05) and promoted smaller values for the maximum plasma concentration (C<sub>max</sub>) and the areas under the curve (AUC<sub>0-480</sub>) with SUF<sub>HP- $\beta$ -CD</sub> (p < 0.05) when compared to SUF. Volume of distribution (V<sub>d</sub>) was higher with SUF<sub>HP- $\beta$ -CD</sub> (p < 0.05) in pigs and rabbits. These results showed that this cyclodextrin-based drug-delivery system of sufentanil was effective to reduce the absorption of the drug.

### Keywords

Mass spectrometry, Absorption, Pharmacokinetics, Opioids, Drug delivery

occur, sufentanil produces less respiratory depressive effects relative to is analgesic effects which justify its use [4].

Development of new medicines is expensive and time consuming so that approaches to improve safety efficacy ratio of "old" drugs have been attempted, such as the use of drug delivery systems [6]. The use of these systems can prolong the effect of the drug or allow the achievement of equivalent effects with lower drug doses. The pharmacokinetics of the drug associated with carriers, such as cyclodextrins, usually shows more constant and lower plasma concentrations when compared to the free drug, suggesting delayed drug transfer to the bloodstream [7].

Previous papers reported that the inclusion complex of sufentanil in 10% hydroxypropyl-beta-cyclodextrin (HP- $\beta$ -CD) increased the effectiveness of sufentanil after epidural and intrathecal administration in rats. After complexation sufentanil is available for a longer period at the spinal level, and, therefore less free sufentanil is available for redistribution, producing less systemic side-effects [8]. In another study, the complexation of sufentanil prolonged the spinal analgesic action and decreased the supraspinal actions of intrathecal drug, due to reduced diffusion into the vascular compartment [9].

A study of our group described a sufentanil-2-HP- $\beta$ -CD inclusion complex that prolonged analgesic effect after intramuscular administration in rats and promoted slow release of SUF after *in vitro* release kinetics tests [10]. Although *in vitro* release tests are convenient, the results obtained may not correspond to the *in vivo* situation. Thus, the objective of this study was to evaluate the pre-clinical pharmacokinetic profile of this new intramuscular formulation of SUF complexed with HP- $\beta$ -CD. Despite of the many therapeutics options, pain is still poorly controlled and might impair everyday activities and quality of life. Our experiment intended to evaluate a new tool in pain control that maybe useful in the future.

### Introduction

Opioids are used for the postoperative period, cancer pain and for moderate to severe chronic noncancer pain [1]. Sufentanil (SUF) is a highly lipophilic opioid that presents rapid and highly effective pain relief [2,3], but it presents short duration of action. Due to this short duration of action, SUF is currently used as an intravenous anesthetic agent and analgesic adjuvant for surgery and labor [4]. SUF produces adverse effects such as bradycardia, respiratory depression or excessive sedation [5]. Even though these adverse effects may

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## Material and Methods

### Preparation of solid inclusion complex

Sufentanil citrate was a gift from Cristália Ind. Farm. Ltda. and HP- $\beta$ -CD were purchased from Roquette Serv. Tech. Lab. The inclusion complex used in this study was identical to that described previously and presented the same *in vitro* characteristics [10]. The complex was obtained by mixing equimolar amounts of HP- $\beta$ -CD and sufentanil (SUF) in deionized water, at room temperature ( $25 \pm 1^\circ\text{C}$ ) for 24 h. After reaching equilibrium, the solution was freeze-dried in a Freezone<sup>®</sup> 4.5L freeze-dry system (Labconco, USA) and stored at  $-20^\circ\text{C}$  for further use. Two milligrams of the solid inclusion complex (SUF<sub>HP- $\beta$ -CD</sub>) were dissolved in 10 mL of HEPES solution (pH 7.40), SUF concentration in the final solution was  $56.2 \mu\text{g}\cdot\text{mL}^{-1}$ .

### Animals and pharmacokinetic study

The experimental protocol was approved by the Institutional Committee for Ethics in Animal Research of São Francisco University (protocol #001.12.09). This randomized blind study was conducted in two independent phases. During Phase I, twelve New Zealand White rabbits (2.50-3.00 kg) were divided into two groups ( $n = 6$ ) and in Phase II ten Landrace pigs (25.00-30.00 kg) were divided into two groups ( $n = 5$ ). The animals were treated by intramuscular route with SUF or SUF<sub>HP- $\beta$ -CD</sub> complex ( $10 \mu\text{g}\cdot\text{kg}^{-1}$ ). The dose used in this study was determinate in pilot study.

In our study design we decided to use two animal species since absorption, distribution and metabolic profile might be diverse in different species. We used the same place of injection and the same technique in both animal species. The place of the injection was the gluteal muscles of pigs and the needle used was a 18 G  $\times$  1 1/2 in. (BD<sup>®</sup>). Rabbits also received the injection in gluteal mass and the needle was a 25 G  $\times$  1 in. (BD<sup>®</sup>). The needle was inserted straight to ensure penetration into the muscle and not in the subcutaneous tissue.

During Phase I and II, an intravascular catheter was inserted in the ear vein of the animals and blood samples (1 mL) were collected via a heparinized cannula pre dose (0 min) and at 15, 30, 45, 60, 90, 120, 180, 240, 300, 360, 420 and 480 minutes after the injection of formulations. These intervals were defined during the pilot study to provide ten samples between the base line (0 min) and approximately 4 times the  $t_{1/2}$  (half-life time) of SUF ( $59.2 \pm 22.0 \text{ min}$ ) [11]. Immediately after each blood collection plasma was separated and stored at  $-70^\circ\text{C}$  until analysis.

### LC-MS/MS assay

Sufentanil plasma levels were determined using a Waters<sup>®</sup> HPLC system (2795) coupled to a Micromass Quattro Premier XE triple stage quadrupole mass spectrometer equipped with an API electrospray source. All separations were carried out on a Phenomenex C18 (100 mm  $\times$  4.6 mm id, 5  $\mu\text{m}$  particle size). The mobile phase was 70% acetonitrile and 30% water with 0.2% formic acid (pH = 3.5). The total run time was 2.5 minutes. The full-scan single-mass spectrum and the daughter ion-mass spectrum for sufentanil and lamivudine (internal standard - IS) were ( $m/z$ )  $387.10 > 238.10$  and  $229.90 > 111.90$ , respectively. The data were integrated using the MassLynx 4.1 (Waters<sup>®</sup>) software. Quality controls samples (QC- 0.15; 48.00 and 96.00  $\text{ng}\cdot\text{mL}^{-1}$ ) were used to validate the method and were prepared by mixing drug-free plasma with appropriate volumes of working solutions.

The frozen plasma samples (200  $\mu\text{L}$ ) were thawed at room temperature and 50  $\mu\text{L}$  of internal standard (IS) (lamivudine 3  $\mu\text{g}/\text{mL}$ ) were added. The samples were vortexed for two minutes and 1000  $\mu\text{L}$  of hexane/ethyl acetate (1:1; V/V) were added. The samples were vortexed for five minutes and centrifuged at  $1200\times g$ , for 5 min at  $-4^\circ\text{C}$ . The organic liquid layer was dried under nitrogen flow. After solvent evaporation, samples were reconstituted in 200  $\mu\text{L}$  mobile phase and 0.15 mL were transferred to LC-MS/MS system vials, for

further injection (5  $\mu\text{L}$ ).

Precision and accuracy of the analytical method were controlled by calculating the intra-batch and inter-batch variation at three concentrations of QC in five replicates ( $n = 5$ ). Three calibration curves were plotted as the peak area ratio versus sufentanil concentration in the range of 0.05-120.00  $\text{ng}\cdot\text{mL}^{-1}$ . The limit of quantification (LQ) was defined as the lowest concentration at which precision and accuracy were within 20% of the true value.

### Pharmacokinetic assessment and statistical analysis

The concentration-time data were analyzed by the noncompartmental approach. The pharmacokinetic parameters were calculated using WinNonlin software (WinNonlin version 5.3, Pharsight Corporation, CA, US). Data were submitted to statistical analysis with unpaired t-test ( $\alpha = 0.05$ ).

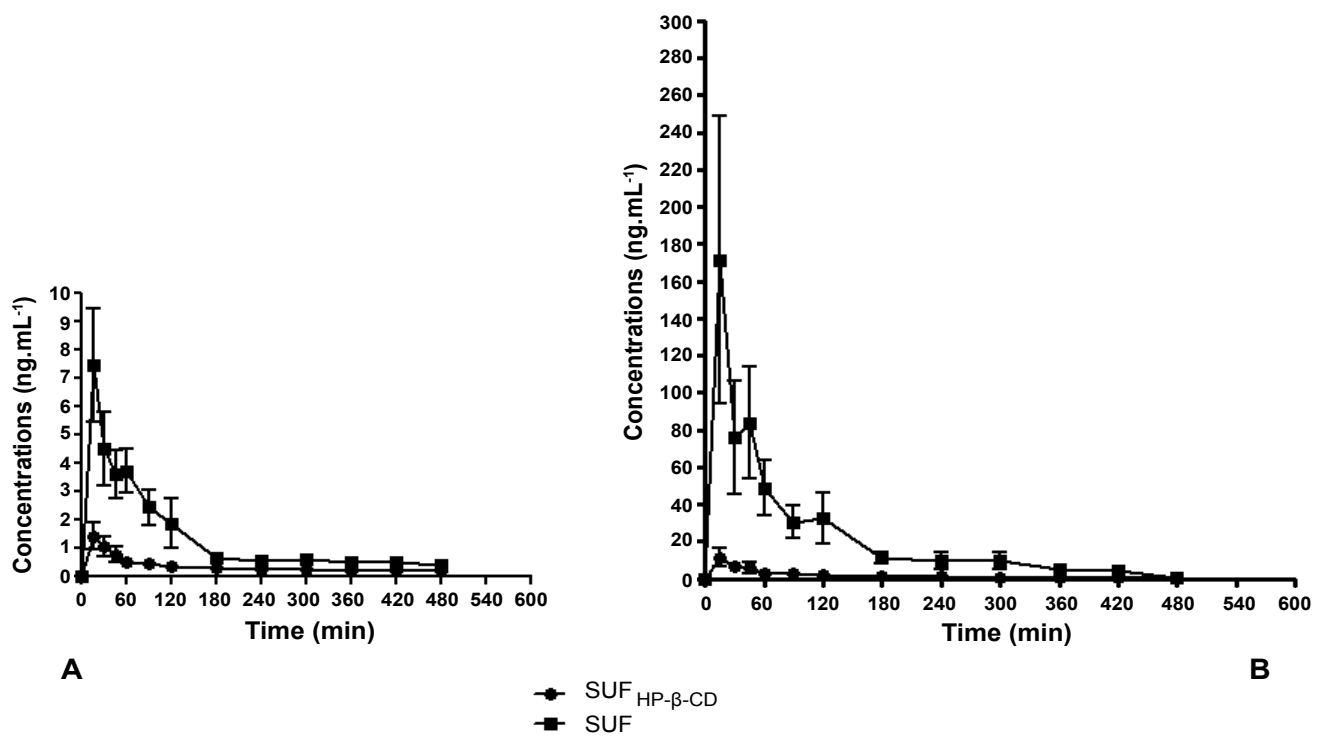
## Results and Discussion

The analysis of SUF was highly selective with the absence of interfering compounds and ion suppression at the retention times for SUF and IS. The calibration curves for SUF showed a good response over the range of 0.05-120.00  $\text{ng}\cdot\text{mL}^{-1}$ . The assay was linear and coefficients ( $r^2$ ) were greater than 0.99 for all curves. Intra and inter-batch accuracy of QC plasma samples ranged from 97.66 to 108.95% and precision ranged from 2.23 to 9.49%. The LQ for SUF was 0.05  $\text{ng}\cdot\text{mL}^{-1}$ . The results indicate that the method is reliable and reproducible within its analytical range.

After the intramuscular administration of the formulations in rabbits, SUF<sub>HP- $\beta$ -CD</sub> induced lower plasma concentrations than SUF at all periods of time ( $p < 0.05$ ), except at 360 min. In pigs, differences in plasma concentrations were observed at almost all periods of time ( $p < 0.05$ ), except at 420 and 480 min. In our study aqueous formulation (SUF) did achieve higher plasma concentrations at almost all the sampling time, but this is not an advantage of the aqueous solution. On the contrary, opioids side effects are related to peak plasma concentrations and drug delivery systems (such as cyclodextrins) could reduce these occurrences [12,13]. All rabbits and pigs presented SUF in the systemic circulation after 15 minutes of the administration of the two formulations.

Previous *in vitro* evaluation of release kinetics showed that SUF<sub>HP- $\beta$ -CD</sub> presents typical characteristics of reduced drug release: indeed total release of SUF was observed at 200 minutes of dialysis, when at the same time just 70% was released from SUF<sub>HP- $\beta$ -CD</sub> (constant release values of  $7.05 \pm 0.52 \text{ min}^{-1/2}$  and  $5.61 \pm 0.39 \text{ min}^{-1/2}$  for SUF<sub>HP- $\beta$ -CD</sub> and SUF, respectively) [10]. The results obtained *in vivo* are in agreement with those. The plasma concentrations of SUF<sub>HP- $\beta$ -CD</sub> after intramuscular administration were more constant and lower when compared to the free drug in almost all periods of time (Figure 1). This reduced absorption to plasma serves as a good indication of the slow-release profile of drugs delivered locally by cyclodextrins [7].

The intramuscular administration of SUF<sub>HP- $\beta$ -CD</sub> and SUF in pigs and rabbits produced huge differences in the pharmacokinetic parameters related to absorption and distribution. In pigs the maximum plasma concentration ( $C_{\text{max}}$ ) values were approximately 24 times bigger in SUF group than in SUF<sub>HP- $\beta$ -CD</sub>. Correspondingly, the areas under the curves ( $AUC_{0-480}$  and  $AUC_{0-\infty}$ ) values were 16 and 12 times bigger in SUF group, respectively. Finally, volume of distribution ( $V_d$ ) values in SUF<sub>HP- $\beta$ -CD</sub> group were 19 times bigger when compared to SUF group. In rabbits the values of  $C_{\text{max}}$ ,  $AUC_{0-480}$  and  $AUC_{0-\infty}$  were around 5; 4 and 2.5 times bigger for SUF, respectively.  $V_d$  was about 7 times bigger for SUF<sub>HP- $\beta$ -CD</sub> (Table 1). These alterations in the pharmacokinetic parameters, especially in the absorption of the drug, could be explained by the fact that complexation with cyclodextrins might change the drug permeation across biologic membranes or its distribution [14,15]. Despite of the absence in differences in  $T_{\text{max}}$  values, our formulation did produce reduced absorption and maintain constant drug concentration during the evaluated time interval. Extended or sustained release formulations are developed to maintain constant or prolonged concentrations of drugs. An



**Figure 1:** Graph of mean plasma concentration versus time after the injection of SUF and SUF<sub>HP-β-CD</sub> complex in rabbits (A) and pigs (B). Values are expressed as mean  $\pm$  SEM. A: differences were observed at all periods of time ( $p < 0.05$ ), except at 360 min; B: differences were observed at all periods of time ( $p < 0.05$ ), except at 420 and 480 min.

**Table 1:** Pharmacokinetic parameters after intramuscular injection of SUF and SUF<sub>HP-β-CD</sub> complex in rabbits and pigs (10  $\mu$ g.kg<sup>-1</sup>). Data expressed as mean ( $\pm$  SD) (n = 5-6/group).

Pharmacokinetic Parameters (Mean $\pm$ SD):	Phase I		Phase II	
	SUF	SUF <sub>HP-β-CD</sub>	SUF	SUF <sub>HP-β-CD</sub>
C <sub>max</sub> (ng.mL <sup>-1</sup> )	7.82 $\pm$ 4.75	1.50 $\pm$ 1.17*	265.97 $\pm$ 297.22	11.29 $\pm$ 8.64*
T <sub>max</sub> (h)	0.41 $\pm$ 0.30	0.29 $\pm$ 0.10	0.35 $\pm$ 0.13	0.45 $\pm$ 0.20
AUC <sub>0-480</sub> (ng-h.mL <sup>-1</sup> )	10.86 $\pm$ 4.44	2.70 $\pm$ 1.83**	215.11 $\pm$ 179.71	13.47 $\pm$ 15.30*
AUC <sub>0-∞</sub> (ng-h.mL <sup>-1</sup> )	12.70 $\pm$ 4.38	4.77 $\pm$ 2.53**	217.47 $\pm$ 178.51	17.12 $\pm$ 22.59*
t <sub>1/2</sub> beta (h)	3.23 $\pm$ 2.08	5.33 $\pm$ 2.55	1.71 $\pm$ 0.79	2.89 $\pm$ 2.07
V <sub>d</sub> (L)	12.89 $\pm$ 10.42	89.57 $\pm$ 75.67*	5.81 $\pm$ 6.37	95.73 $\pm$ 58.70**

**Note:** Statistical Analysis: Phase I- SUF vs. SUF<sub>HP-β-CD</sub>:  $p < 0.01$ [\*\*],  $p < 0.05$ [\*],  $p > 0.05$  [not significant];

Phase II- SUF vs. SUF<sub>HP-β-CD</sub>:  $p < 0.01$ [\*\*],  $p < 0.05$ [\*],  $p > 0.05$  [not significant]. C<sub>max</sub>- Maximum Plasma Concentration; T<sub>max</sub>: Time to reach maximum plasma concentration; AUC: Areas under the curves; t<sub>1/2</sub>: Half life of elimination; V<sub>d</sub>: Volume of distribution.

ideal opioid extended release formulation would provide consistent pain control and minimization of adverse events associated with peak drug levels. Distinct technologies of formulations for opioids might produce varied release and pharmacokinetic profiles. The pharmacokinetic profile might present no lag time in drug absorption and exhibited a plasma concentration versus time profile with a sharp initial slope similar to immediate-release formulations followed by a sustained release phase [13], as our formulation behavior. Our group proposed a new formulation of sufentanil complexed with cyclodextrins designed for intramuscular use. We designed this study with two animal species to collect fundamental pre-clinical data in order to allow clinical evaluation in the future. Pigs and rabbits are good options to perform pharmacokinetic studies, especially because these animals present a higher volume of blood and easy ways to collect it when compared to rats. Also we decided to use "large experimental animal models" to observe extensive whole-body pharmacokinetics in a context comparable to patient physiology [16]. We observed that this new formulation was able to reduce the release and the absorption of SUF. Thus, the use of HP-β-CD may be an interesting strategy to diminish the liberation of SUF after intramuscular administration.

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